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Hearing and Speech Perception for People With Hearing Loss Using Personal Sound Amplification Products

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ABSTRACT

Background: Hearing loss (HL) is the most common chronic disease and has been linked to negative health outcomes. Hearing aids (HAs) are regarded as the gold standard for HL management, however, the adoption rate of HAs is relatively low for various reasons. With this background, hearing devices, such as personal sound amplification products (PSAPs) received significant attention as an alternative to conventional HAs. This study aimed to evaluate the clinical efficacy of PSAPs in patients with mild to moderately severe HL.

Methods: Nineteen patients with mild hearing loss (MHL), 23 with moderate hearing loss (MDHL), and 15 with moderately severe hearing loss (MSHL) participated in the study. Electroacoustic analysis, simulated real-ear measurements (REMs), and three clinical evaluations were implemented.

Results: All devices satisfied the electroacoustic tolerances. All devices provided sufficient gain for MHL and MDHL audiograms. However, in MSHL audiogram, the gains of PSAPs were insufficient, especially for high frequencies. In terms of clinical evaluations, sound-field audiometry showed significant improvements between aided and unaided thresholds in all groups for all devices ($P < 0.001$). Significant improvements of word recognition scores were only shown for HAs between aided and unaided conditions. The Korean version of the Hearing In Noise Test did not show any consistent findings for all devices and groups.

Conclusion: Certain PSAPs are beneficial for improving hearing and speech perception in patients with HL. Well-chosen PSAPs could be an alternative hearing rehabilitation option for these patients.

Keywords: Hearing Loss; Hearing Aids; Personal Sound Amplification Products; Wearable Electronic Devices

INTRODUCTION

The World Health Organization reported in 2020 that approximately 5% of the world's population has hearing loss (HL), and it is expected that one in 10 individuals will develop HL due to the rapidly aging population.¹ HL is the third most prevalent chronic condition

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Author Contributions

Conceptualization: Kim GY, Jo M, Seol HY, Cho YS. Data curation: Kim GY, Kim S, Lim J. Formal analysis: Kim GY, Kim S, Lim J. Funding acquisition: Moon IJ. Investigation: Kim GY, Jo M. Methodology: Kim GY, Jo M, Cho YS. Project administration: Kim GY. Supervision: Moon IJ. Visualization: Kim GY. Writing – original draft: Kim GY, Kim S, Jo M, Seol HY, Cho YS, Moon IJ. Writing – review & editing: Kim GY, Kim S, Seol HY, Cho YS, Lim J, Moon IJ.

faced by older adults² and has been linked to negative health outcomes including depressive symptoms,³ decreased quality of life,⁴ and cognitive deficits.⁵ Recent evidence suggests that HL is a significant modifiable risk factor against dementia,⁶ therefore, proactive hearing rehabilitation is essential.

Previous studies have demonstrated that untreated HL increases the burden of health care costs and health care system utilization.⁷ However, when the access to hearing care services with hearing aids (HAs), value to the healthcare system are added and Medicare spending is reduced.⁸ Nonetheless, the adoption rate of HAs is relatively low, at 34.1% for all individuals reporting hearing difficulty.⁹ The main reasons for the low uptake rate of HAs are high costs and stigma.⁹ Therefore, hearing devices, such as over-the-counter (OTC) devices including personal sound amplification products (PSAPs) received significant attention as an alternative to conventional HAs.

The reports from the President's Council of Advisors on Science and Technology (PCAST) and the National Academies of Sciences, Engineering, and Medicine (NASEM) emphasized HL as being a public health concern and underlined the need for policy changes to increase accessibility and affordability of hearing care.^{10,11} One of the ways is to advocate use of OTC devices in addition to HAs for those with mild to moderate HL. Up to now, however, OTC devices are unregulated by the US FDA¹² and there is insufficient evidence for clinical benefit.

The purpose of this study was to explore the effectiveness of PSAPs based on the following three aims: 1) verification of device specification through electroacoustic testing, 2) evaluation of amplification through simulated real-ear measurements (REMs), and 3) comparison of unaided and aided performance based on two HAs and two PSAPs.

METHODS

Participants

A total of 57 patients with HL participated in the study. All patients visited the outpatient clinic of the Department of Otorhinolaryngology between March 2019 and May 2020. All patients got briefed information about the research, and those who agreed to participate signed informed consent before the study started. Inclusion criteria were as follows: 1) age 19 years or older, 2) mentally and physically able to participate in this study, 3) HL of 26 dB or more based on four frequency averages (0.5, 1, 2, and 4 kHz) in both ears, 4) no history of neurological, cognitive, learning, or language disorder at the time of informed consent, and 5) speaks Korean as a first language. Patients were divided into three groups based on the averages of four frequencies (0.5, 1, 2, and 4 kHz) of both ears, patients were divided into three groups: mild hearing loss (MHL) (26–40 dB HL), moderate hearing loss (MDHL) (41–55 dB HL), and moderately severe hearing loss (MSHL) (56–70 dB HL). In this study, 19, 23, and 15 patients were included in the MHL, MDHL, and MSHL, respectively. The participants' characteristics are shown in **Table 1**.

Hearing devices

Two HAs and two PSAPs were chosen based on popularity, availability, and type. The LiNX 3D (GN Hearing A/S, Ballerup, Denmark) was chosen as the premium HA, and the Nevara1 (Bernafon AG, Bern, Switzerland) was used as the basic HA. The premium HA has 12 channels with additional functions, and the basic HA has only 6 channels. In the case of

Table 1. Participant characteristics

| Characteristics | MHL (n = 19) | MDHL (n = 23) | MSHL (n = 15) | P value |
|--|---------------------|--------------------|--------------------|------------|
| Age, median (IQR), yr | 58 (39–62) | 60 (53–64) | 55 (28–61) | 0.183 |
| Male, No. (%) | 7 (36.8) | 13 (56.5) | 7 (46.7) | 0.445 |
| PTA, median (IQR), dB HL | | | | |
| AC, right | 37.5 (30–40) | 42.5 (41.25–48.75) | 60 (56.25–62.5) | < 0.001*** |
| AC, left | 36.25 (33.75–38.75) | 47.5 (41.25–55) | 63.75 (57.5–66.25) | < 0.001*** |
| Previous HA experience, No. (%) ^a | 3 (15.8) | 7 (30.4) | 8 (53.3) | 0.064 |

MHL = mild hearing loss, MDHL = moderate hearing loss, MSHL = moderately severe hearing loss, IQR = inter-quartile range, PTA = pure-tone average, AC = air conduction, HA = hearing aid.

^aOnly HA experience longer than 3 months is reported.

***P < 0.001.

the PSAPs, the CS50+ (Sound World Solutions, IL, USA) was chosen as the premium PSAP, and the Etymotic Bean (Etymotic Research Inc., IL, USA) was used as the basic PSAP. The premium PSAP has 16 channels and allows user to customize sounds to their amplification preferences and environments. The basic PSAP offers only two levels of enhancement. The HA fittings were performed by experienced audiologists using the National Acoustics Laboratories-Non-Linear prescription, the 2nd generation (NAL-NL2) formula. For the premium PSAP, self-fitting is possible through a dedicated smartphone application. As with the basic PSAP, the participants selected their preferred amplification mode from among the two presets (normal and high). The features of each device are described in **Table 2**.

Outcome measures

This study was composed of three phases: 1) electroacoustic analysis, 2) simulated REMs, and 3) clinical evaluations.

Electroacoustic analysis

Electroacoustic analysis was carried out using the Aurical Hearing Instrument Test (HIT) box and OTOSuite software (GN Otometrics A/S, Ballerup, Denmark) based on ANSI S3.22 standards to determine the quality of the devices. Tests were established according to previous research¹³⁻¹⁶ including maximum output sound pressure level at 90 dB SPL (OSPL 90), frequency range, equivalent input noise (EIN), and total harmonic distortion (THD). The procedures and tolerances for each test are described below.

- OSPL 90: OSPL 90 was measured with a 90-dB SPL pure-tone sweep (0.25–5 kHz) with devices on the full-on-gain setting. OSPL 90 should not exceed 120 dB SPL.¹⁴⁻¹⁶
- Frequency range: Frequency range was measured in the reference test gain setting and refers to the range between the lowest frequency and the highest frequency at which the response curve is 20 dB below its high-frequency average output sound pressure level. We assessed whether the frequency of speech (0.25–6 kHz) was included in each device’s frequency range.¹³⁻¹⁷
- EIN: The level of internal noise that can be caused by the transmitter and amplifier was measured for EIN. EIN tolerance should be less than 28 dB SPL.^{13-16,18}

Table 2. Features of each hearing device

| Devices | Model No. | Manufacturer | Retail cost | Type | Channel |
|----------------------|-----------|-------------------------|---------------|------|---------|
| LiNX 3D (premium HA) | LT561-DRW | GN Hearing A/S | \$1,699/each | RIC | 12 |
| Nevara1 (basic HA) | E072007 | Bernafon | \$995/each | ITC | 6 |
| CS50+ (premium PSAP) | CS50+ | Sound world Solution | \$349.99/each | BTE | 16 |
| Bean (basic PSAP) | Bean | Etymotic Research, Inc. | \$299.99/each | ITE | - |

HA = hearing aid, RIC = receiver-in-the-ear, ITC = in-the-canal, PSAP = personal sound amplification product, BTE = behind-the-ear, ITE = in-the-ear.

- THD: The input sound pressure of 500, 800, and 1,600 Hz pure tones was used to measure THD. Harmonic distortion can occur due to peak clipping or the electrical circuit of the amplifier. THD should be within 3%.¹³⁻¹⁸

Simulated REMs

The second phase of the study examined simulated REMs with a 2-cc coupler to evaluate whether the devices provided an appropriate amount of amplification. Target gain, calculated by a fitting formula for three virtual audiograms, and real-ear insertion gain (REIG), calculated through REMs, was compared. The three virtual audiograms were set to the average hearing thresholds of each HL group (Fig. 1). Once the device was placed in the Aurical HIT text box, the International Speech Test Signal (ISTS) at 65 dB SPL was presented, and the gain calculated by fitting formula and REIG was compared. The NAL-NL2 was used. The amount of amplification was considered appropriate if the difference between the target gain and REIG was within 10 dB at five or more of seven frequencies (0.25, 0.5, 1, 2, 3, 4, and 6 kHz).¹³⁻¹⁶

Clinical evaluations

Three main test batteries were administered: 1) sound-field audiometry, 2) word recognition scores (WRS), and 3) the Korean version of the Hearing In Noise Test (K-HINT).

First, unaided and aided sound-field thresholds were obtained. A warble tone of 0.25–6 kHz was presented through a loudspeaker located 1 m from the patient. The 4-frequency averages (0.5, 1, 2, and 4 kHz) for each device were calculated for comparison.

Second, the patient's speech perception with and without the device was evaluated through the WRS. Twenty-five monosyllabic words from the Korean standard-monosyllabic word list (KS-MWL-A)¹⁹ were presented at 65 dB HL through a loudspeaker located 1 m from the patient. The patient was asked to repeat the word back to the tester. Percent-correct scores were calculated for scoring.

Third, K-HINT was performed to assess the patient's speech recognition in noise.²⁰ Speech spectrum noise was presented through the loudspeaker at a fixed level of 65 dBA. The presentation level of the target speech was adjusted to measure a signal-to-noise ratio (SNR) at which the patient recognized the sentences 50% of the time. The higher was the SNR, the more difficult the patient had hearing in noise.

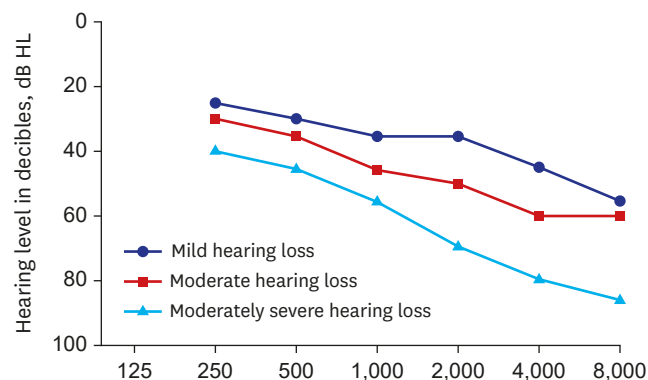


Fig. 1. Three virtual audiograms for real-ear measurements.

Statistical analysis

Using descriptive statistical analysis, median and interquartile range (IQR) were used for continuous variables, while numbers and percentages were used for categorical variables. The Friedman test was used to compare clinical outcomes between the five conditions. The Wilcoxon signed-rank test was conducted as a post-hoc analysis. The Bonferroni correction was applied to account for multiple testing. All statistical analyses were completed using SPSS ver. 25.0 (IBM Corp., Armonk, NY, USA).

Ethics statement

This study was approved by the Institutional Review Board (IRB) of Samsung Medical Center and the requirement for informed consent was waived (IRB No. 2018-11-117).

RESULTS

Electroacoustic analysis

All devices showed satisfactory performances in four measurements (OSPL 90, frequency range, EIN, and THD). Regarding the OSPL 90, all four devices were within the tolerance limits (< 120 dB SPL). As for the frequency range, all four devices met the tolerance (250–6,000 Hz). For EIN, all four devices were within the acceptance tolerance (< 28 dB SPL). All four devices also showed appropriate tolerance value for the THD (< 3%) (Table 3)

Simulated REMs

For three virtual audiograms, all devices showed an appropriate amount of amplification; the difference between the fitting formula and REIG was within 10 dB at five or more frequencies. However, as for the moderately severe HL, all PSAPs demonstrated a lack of amplification at high frequencies (Fig. 2).

Clinical evaluations

Sound field audiometry

All devices showed significant improvements between aided and unaided thresholds in all groups (Table 4).

WRS

For the MHL group, the premium HA ($P = 0.024$) and the basic HA ($P < 0.001$) showed significant improvements between aided and unaided conditions. In the MDHL group, the premium HA ($P < 0.001$), the basic HA ($P < 0.001$), and the basic PSAP ($P = 0.027$) revealed significant improvements between aided and unaided conditions. In the MSHL group, all devices demonstrated significant improvements between aided and unaided conditions (Table 4).

Table 3. Electroacoustic analysis of the hearing devices included in the study

| Devices | Electroacoustic analysis results ^a | | | | | |
|----------------------|---|----------------------|--------------|---------|--------|----------|
| | OSPL 90 (dB SPL) | Frequency range (Hz) | EIN (dB SPL) | THD (%) | | |
| | | | | 500 Hz | 800 Hz | 1,600 Hz |
| LiNX 3D (premium HA) | 113.8 | 100–7,157.2 | 26.3 | 0.9 | 0.8 | 0.5 |
| Nevara1 (basic HA) | 110.7 | 100–6,615.6 | 26.7 | 0.4 | 0.5 | 2.2 |
| CS50 (premium PSAP) | 118.3 | 103–6,903 | 27 | 2 | 1.5 | 0.4 |
| Bean (basic PSAP) | 97.9 | 118–6,691 | 22.4 | 0.7 | 0.7 | 0.7 |

OSPL 90 = output sound pressure level for 90 dB input sound pressure level, SPL = sound pressure level, EIN = equivalent input noise, THD = total harmonic distortion, HA = hearing aid, PSAP = personal sound amplification product.

^aTolerances described in *Methods* were applied: OSPL90, < 120 dB SPL; frequency range, 250–6,000 Hz; EIN, < 28 dB SPL; THD, < 3%.

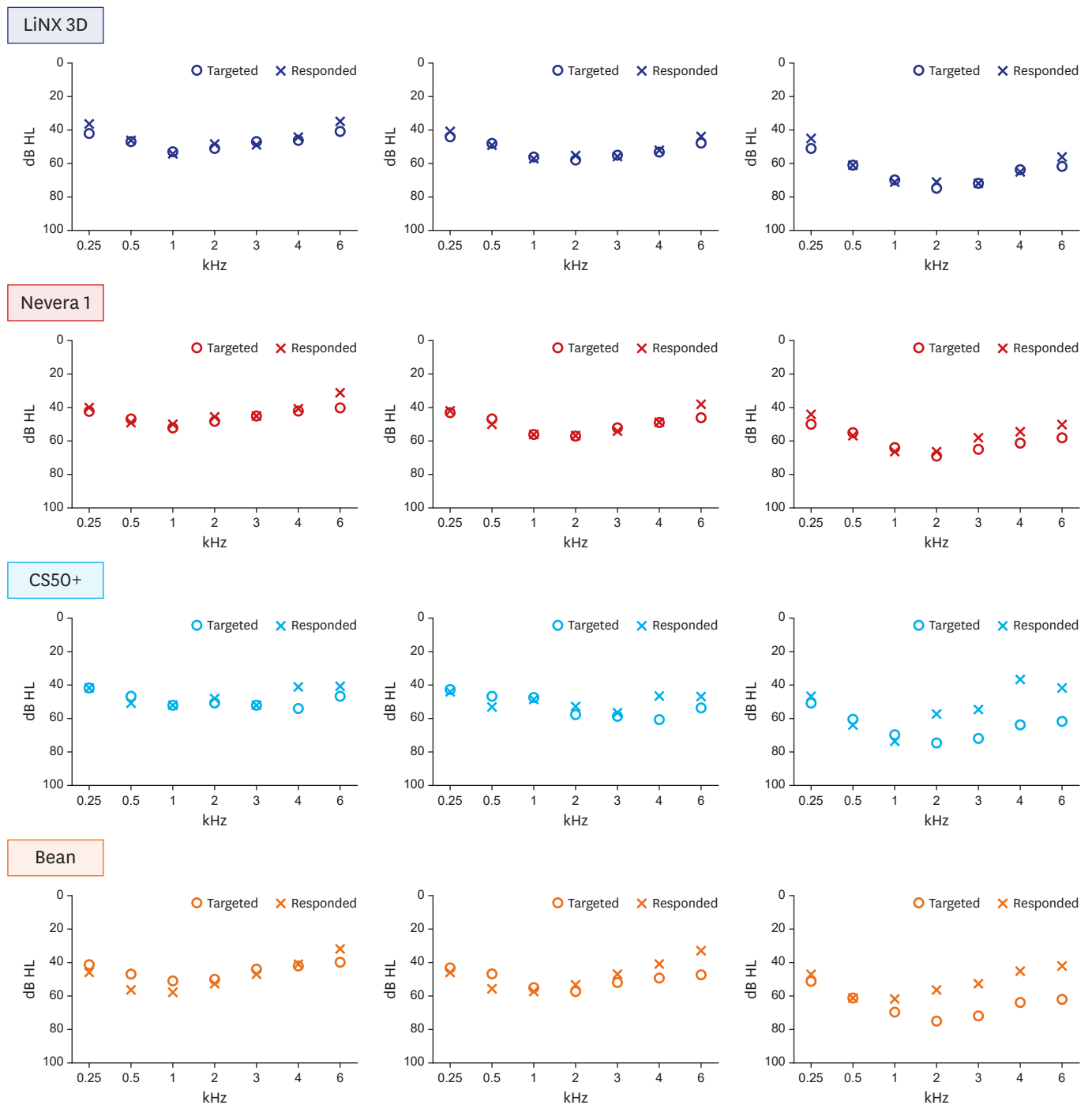


Fig. 2. Simulated real-ear measurement results.

K-HINT

For the MHL group, all devices showed significant changes between aided and unaided conditions. In the MDHL group, the premium PSAP ($P = 0.021$) and the basic PSAP ($P = 0.011$) revealed significant improvements between aided and unaided conditions. In the MSHL group, the basic HA ($P = 0.001$) and the basic PSAP demonstrated significant improvements between aided and unaided conditions (Table 4).

Table 4. Clinical evaluation results

| Measures | Group | Test results, Median (IQR) | | | | | P value | Post-hoc analysis ^a | | | |
|--------------------------------|-------|----------------------------|----------------------|------------------------|------------------------|-------------------------|------------|--------------------------------|---------------------|-------------------|------------------|
| | | Unaided | LiNX 3D (premium HA) | Nevara1 (basic HA) | CS50+ (premium PSAP) | Bean (basic PSAP) | | Unaided vs. LiNX 3D | Unaided vs. Nevara1 | Unaided vs. CS50+ | Unaided vs. Bean |
| Sound-filed audiometry (dB HL) | MHL | 40.625 (38.75, 43.75) | 31.25 (28.75, 35) | 36.625 (32.5, 40) | 31.875 (30, 36.25) | 30.625 (28.75, 32.5) | < 0.001*** | < 0.001*** | < 0.001*** | 0.002** | < 0.001*** |
| | MDHL | 48.75 (45, 55) | 35 (32.4, 40) | 45 (41.25, 50) | 40.625 (35, 45) | 37.5 (33.75, 42.5) | < 0.001*** | < 0.001*** | < 0.001*** | < 0.001*** | < 0.001*** |
| | MSHL | 65 (58.75, 71.25) | 45 (41.25, 51.25) | 57.5 (53.75, 63.75) | 48.75 (42.5, 53.75) | 47.5 (45, 55) | < 0.001*** | < 0.001*** | < 0.001*** | < 0.001*** | < 0.001*** |
| WRS (%) | MHL | 92 (92, 96) | 96 (92, 96) | 92 (92, 96) | 92 (84, 96) | 96 (96, 100) | 0.005** | 0.024* | < 0.001*** | 1.000 | 0.177 |
| | MDHL | 88 (80, 92) | 92 (84, 96) | 88 (84, 92) | 84 (80, 96) | 92 (84, 96) | 0.001** | < 0.001*** | < 0.001*** | 1.000 | 0.027* |
| | MSHL | 60 (24, 68) | 88 (52, 92) | 76 (40, 84) | 68 (52, 88) | 80 (52, 92) | < 0.001*** | < 0.001*** | < 0.001*** | 0.004** | < 0.001*** |
| K-HINT (SNR) | MHL | -0.7 (-1.8, 0.3) | -0.6 (-1.6, 1) | 1.4 (-0.3, 2.4) | -0.2 (-1.6, 0.5) | -0.5 (-1.1, 0.3) | 0.053 | 0.002** | < 0.001*** | < 0.001*** | < 0.001*** |
| | MDHL | 1 (-0.1, 2.8) | 0.9 (-0.7, 3.8) | 1.4 (-0.1, 2.8) | -0.1 (-1.8, 1.9) | -0.4 (-1.3, 1.3) | 0.007** | > 0.99 | > 0.99 | 0.021* | 0.011* |
| | MSHL | 4.7 (2.6, 12.1) | 5.1 (1.8, 10) | 3.3 (2.2, 7.4) | 3 (0.7, 10.8) | 3.3 (0.8, 6) | 0.002** | 0.202 | 0.002** | 0.179 | 0.001** |

IQR = inter-quartile range, HA = hearing aid, PSAP = personal sound amplification product, MHL = mild hearing loss, MDHL = moderate hearing loss, MSHL = moderately severe hearing loss, WRS = word recognition score, K-HINT = Korean version of the Hearing In Noise Test.

^aThe comparison result of each device was corrected by the Bonferroni correction method for type I error increase by multiple comparisons.

*P < 0.05, **P < 0.01, ***P < 0.001.

DISCUSSION

Our study investigated the effectiveness of four hearing devices using electroacoustic testing, simulated REMs, and clinical evaluations, including sound-field audiometry, WRS, and K-HINT. All devices satisfied the four tolerances for the electroacoustic properties of OSPL 90, frequency range, EIN and THD. All devices provided an adequate amount of amplification for the MHL and MDHL virtual audiograms. However, in MSHL audiogram, the gain was insufficient, especially for high frequencies when using PSAPs. Therefore, it is considered that conventional HAs are more appropriate to the patients with MSHL than the PSAPs. Regarding the sound-field audiometry, all devices showed significant improvement between aided and unaided thresholds in all groups. Significant improvements of WRS were only shown for HAs between aided and unaided conditions. K-HINT did not show any consistent findings for all devices and groups.

The devices that met the tolerances for electroacoustic properties suggest that PSAPs in the study showed comparable electroacoustic performance to HAs. Quality control is performed systematically for HAs based on technical specification sheets of IEC and ANSI standards available from their manufacturers. Product quality, however, varies for PSAPs,¹⁸ and it is difficult to perform quality control as they do not have specification sheets. Therefore, it is necessary to closely examine the quality of these devices.

Manchaiah et al.¹⁸ claimed OSPL 90, EIN, and THD as the most important factors for assessing the quality of OTC products. Considering that OTC devices would mostly be used by individuals with mild and moderate HL, OSPL 90, in particular, needs to be verified (> 120 dB SPL) to prevent further HL. Additionally, issues, such as feedback and noise must be addressed.¹⁸ Some studies reported higher EIN values for low-end OTC devices,^{13,17} but PSAPs used in the study had EIN values within the tolerances set by ANSI (< 28 dB SPL). Higher internal noise can interfere with one's ability to recognize target speech. THD for most OTC devices as well as all devices investigated in the present study were below the ANSI standard of 3%.^{13,18}

Simulated REMs illustrated that all devices provided sufficient gain for the MHL and MDHL audiograms based on the NAL-NL2 formula. However, in moderately severe HL, the gain was insufficient for high frequencies. These results are consistent with prior research showing that the functionality of PSAPs is not sufficient for moderately severe HL.²¹⁻²³ The low gain of high frequencies leads to problems with speech perception. Therefore, HAs that can sufficiently amplify high frequencies are more suitable for those with moderately severe HL.

Comparing aided and unaided sound-field thresholds, all devices showed a significant decrease in hearing thresholds at all frequencies in all groups.²¹ The WRS significantly improved in all groups with HAs. The reason for no significant differences between aided and unaided conditions with PSAPs could be due to a ceiling effect. For instance, the median WRS for the unaided and premium PSAP conditions was 92% in the MHL group.

For K-HINT, no consistent results were obtained for all groups and devices.¹⁶ One probable explanation is that PSAPs equally amplify all frequencies, meaning that both speech and noise were louder. Therefore, hearing devices amplified both noise and speech at the same level, offering no assistance to patients in distinguishing the two.

Though interest in PSAPs has increased around the world, many people remain unfamiliar with the devices.⁹ In addition, 65% of patients with HL will purchase an HA through hearing healthcare professionals, even though they can purchase OTC devices.⁹ This result suggests that patients have stronger confidence in HA than in OTC devices. In the study, certain PSAPs were effective for assisting communication in all three HL groups. Therefore, well-chosen PSAPs can be helpful for communication in daily life. An educational and awareness campaign for PSAPs will be necessary in an attempt to increase the accessibility and affordability of hearing rehabilitation. However, the PSAPs selected in the study do not represent all PSAPs available in the market. Thus, the government needs to prepare guidelines for OTC devices, including PSAPs, to control device quality.

There are some limitations to the study. For example, the REMs were not performed on individual patients. In the future, clinical evaluation after REMs would lend to accurate results.

Findings of the study demonstrated PSAPs were beneficial in improving hearing and speech perception in patients with HL. The results suggest that well-chosen PSAPs that were verified through electroacoustic analysis, REMs, and clinical evaluations can be used as an alternative hearing rehabilitation option for people affected by HL.

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